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13 Noise, balanced feedback networks, synaptic scaling, and linear response. Part 2

13.1 Circuit model

So far we have only address noise and scaling at the level of noise in individual cells. Now we analyze a network of neurons with balanced inputs (Figure 1). We consider the consequences of the choice of connections in a network on the ability to maintain the balanced state.



Consider a network of a population of interconnected excitatory (E) and inhibitory (I) cells. The full equations are

$$\tau_E \frac{dV_i^E(t)}{dt} + V_i^E(t) = \left[\beta(\mu_i^E(t) - \theta_i^E)\right]_+$$
(13.1)

and

$$\tau_{I} \frac{dV_{i}^{I}(t)}{dt} + V_{i}^{I}(t) = \left[\beta(\mu_{i}^{I}(t) - \theta_{i}^{I})\right]_{+}, \qquad (13.2)$$

where $[\cdot \cdot \cdot]_+$ is the Heavyside function, τ_E and τ_I are the cellular time constant, β is the conversion gain, and the θ_i^E and θ_i^I are

thresholds. The inputs are

$$\mu_i^E(t) = \mu_{ext}^E(t) + \sum_{j=1}^K W_{i,j}^{EE} V_j^E(t) + \sum_{j=1}^K W_{i,j}^{EI} V_j^I(t)$$
(13.3)

and

$$\mu_i^I(t) = \mu_{ext}^I(t) + \sum_{j=1}^K W_{i,j}^{II} V_j^I(t) + \sum_{j=1}^K W_{i,j}^{IE} V_j^E(t).$$
(13.4)

As in the case of the model cell, we will scale the synaptic inputs by $1/\sqrt{K}$, as opposed to 1/K, i.e.,

$$W_{ij}^{EE} \to \frac{W^{EE}}{\sqrt{K}}; \quad W_{ij}^{II} \to -\frac{W^{II}}{\sqrt{K}}; \quad W_{ij}^{EI} \to -\frac{W^{EI}}{\sqrt{K}}; \quad W_{ij}^{IE} \to \frac{W^{IE}}{\sqrt{K}}$$
(13.5)

where we explicitly put in the negative signs of inhibition. As will soon be clear, we need to scale the external inputs by

$$\mu_{ext}^E(t) \to \sqrt{K} \ E \ m_{ext}(t) \quad \text{and} \quad \mu_{ext}^I(t) \to \sqrt{K} \ I \ m_{ext}(t) \quad (13.6)$$

where E and I are inputs of strength of O(1). The dependence on a common term is a statement that excitatory and inhibitory neurons share the same tuning curve. All together, we have

$$\mu_i^E(t) = \sqrt{K} E m_{ext}(t) + \frac{W^{EE}}{\sqrt{K}} \sum_{j=1}^K V_j^E(t) - \frac{W^{EI}}{\sqrt{K}} \sum_{j=1}^K V_j^I(t) \quad (13.7)$$

and

$$\mu_i^I(t) = \sqrt{K} Im_{ext}(t) + \frac{W^{IE}}{\sqrt{K}} \sum_{j=1}^K V_j^E(t) - \frac{W^{II}}{\sqrt{K}} \sum_{j=1}^K V_j^I(t). \quad (13.8)$$

In terms of the order parameters,

$$\mu_{E}(t) = \sqrt{K}Em_{ext}(t) + \sqrt{K}W^{EE}\frac{1}{K}\sum_{j=1}^{K}V_{j}^{E}(t) - \sqrt{K}W^{EI}\frac{1}{K}\sum_{j=1}^{K}V_{j}^{I}(t)$$

$$= \sqrt{K}Em_{ext}(t) + \sqrt{K}W^{EE}m_{E}(t) - \sqrt{K}W^{EI}m_{I}(t) \qquad (13.9)$$

$$= \sqrt{K}\left[Em_{ext}(t) + W^{EE}m_{E}(t) - W^{EI}m_{I}(t)\right]$$

and

$$\mu_{I}(t) = \sqrt{K} I m_{ext}(t) + \sqrt{K} W^{IE} \frac{1}{K} \sum_{j=1}^{K} V_{j}^{E}(t) - \sqrt{K} W^{II} \frac{1}{K} \sum_{j=1}^{K} V_{j}^{I}(t)$$

$$= \sqrt{K} \left[I m_{ext}(t) + W^{IE} m_{E}(t) - W^{II} m_{I}(t) \right].$$
(13.10)

As $\sqrt{K} \to \infty$ the left hand side goes to zero and the equilibrium state will satisfy

$$0\left(\frac{1}{\sqrt{K}}\right) = Em_{ext}(t) + W^{EE}m_E(t) - W^{EI}m_I(t)$$
 (13.11)

and

$$0\left(\frac{1}{\sqrt{K}}\right) = Im_{ext}(t) + W^{IE}m_{E}(t) - W^{II}m_{I}(t).$$
(13.12)

The implication of this equilibrium condition is that the average input remains finite as the fluctuations remain large (Figures 2 and 3). This is the balanced state.

Figure 2: Balanced networks have emergent variability. From Shadlen and Newsome, 1994.



Figure 3: Statistics of have emergent variability. From Shadlen and Newsome, 1994.



13.2 The balanced state

Solving the above equations for m_E^o and m_I^o gives relations for the equilibrium activity of the excitatory and inhibitory cells in terms of the external drive:

$$m_E^0 = \frac{W^{II}E - W^{EI}I}{W^{EE}W^{II} - W^{EI}W^{IE}}m_{ext}.$$
 (13.13)

$$m_I^0 = \frac{W^{IE} E - W^{EE} I}{W^{EE} W^{II} - W^{EI} W^{IE}} m_{ext}.$$
 (13.14)

Recall that the equilibrium values of activity m_E^o and m_I^o must be both positive and bounded by 1. This constrains the values of the synaptic weights.

13.2.1 Linear response

A seemingly paradoxical effect is that increasing the external inhibitory input, i.e., increasing I, will lead to a net decreased spiking of inhibitory cells and lwill concurrently decrease both m_E and m_I (Figure 4). This is a feedback effect. Excitatory and inhibitory activity track each other until the excitatory cells are completely turned off; this behavior is seen across cortical regions (Figure 5).

Figure 4: Experimental set-up to study linear response of network as we drive inhibition. From Sanzeni, Akitake, Goldbach, Leedy, Brunel and Histed 2020.



Figure 5: Linear response, until stauration, of network as we drive inhibition. From Sanzeni, Akitake, Goldbach, Leedy, Brunel and Histed 2020.



A second issue is that rapid feedback prevents the occurence of significant correlations. This depends of having faster inhibitory than excitatory synapses, as occurs for Gaba-A, but not Gaba-B (Figure ??).

13.2.2 Stability and response speed

We return to the full network equations and look at the variation around the equilibrium value of m_E and m_I . Taking the time constants, τ , conversion gains, β , and thresholds to be the same for the *E* and *I* populations, and denoting

$$\delta m_E(t) = m_E(t) - m_E^o \tag{13.15}$$

and

$$\delta m_I(t) = m_I(t) - m_I^o \tag{13.16}$$

leads to

$$\tau \frac{d \,\delta m_E(t)}{dt} + \delta m_E(t) = \left[\beta \sqrt{K} \left(W^{EE} \delta m_E(t) - W^{EI} \delta m_I(t) \right) \right]_+$$
(13.17)

and

$$\tau \frac{d \,\delta m_I(t)}{dt} + \delta m_I(t) = \left[\beta \sqrt{K} \left(W^{IE} \delta m_E(t) - W^{II} \delta m_I(t) \right) \right]_+.$$
(13.18)

When the neurons are active, this reduces to the linear equations

$$\tau \frac{d \,\delta m_E(t)}{dt} + \delta m_E(t) = \beta \sqrt{K} \left(W^{EE} \delta m_E(t) - W^{EI} \delta m_I(t) \right)$$
(13.19)

and

$$\tau \frac{d \,\delta m_I(t)}{dt} + \delta m_I(t) = \beta \sqrt{K} \left(W^{IE} \delta m_E(t) - W^{II} \delta m_I(t) \right).$$
(13.20)

These linear equations are solved by taking $\delta m_E(t) \propto e^{\lambda t}$, so that

$$(\lambda \tau + 1) \,\delta m_E(t) = \beta \sqrt{K} \left(W^{EE} \delta m_E(t) - W^{EI} \delta m_I(t) \right) \quad (13.21)$$

and

$$(\lambda \tau + 1) \,\delta m_I(t) = \beta \sqrt{K} \left(W^{IE} \delta m_E(t) - W^{II} \delta m_I(t) \right), \quad (13.22)$$

which requires that

$$\begin{cases} \beta \sqrt{K} W^{EE} - 1 - \lambda \tau & -\beta \sqrt{K} W^{EI} \\ \beta \sqrt{K} W^{IE} & -\beta \sqrt{K} W^{II} - 1 - \lambda \tau \end{cases} = 0 \quad (13.23)$$

and leads to

$$\lambda_{1,2} = \frac{\beta\sqrt{K}\left(W^{EE} - W^{II}\right) - 2}{2\tau}$$

$$\pm \frac{1}{\tau}\sqrt{\left(\frac{\beta\sqrt{K}\left(W^{EE} - W^{II}\right) - 2}{2}\right)^2 - \beta^2 K W^{IE} W^{EI}}$$

$$\overrightarrow{K \to \infty} \quad \frac{\beta\sqrt{K}}{\tau} \left[\frac{W^{EE} - W^{II}}{2} \pm \sqrt{\left(\frac{W^{EE} - W^{II}}{2}\right)^2 - W^{IE} W^{EI}}\right]$$

$$= \frac{\beta\sqrt{K}}{\tau} \left[\frac{W^{EE} - W^{II}}{2}\right] \left[1 \pm \sqrt{\left(1 - 4\frac{W^{IE} W^{EI}}{W^{EE} - W^{II}\right)^2}\right)}\right].$$

The system is stable only if the real part of $\lambda_{1,2} < 0$. This implies

$$W^{II} > W^{EE}, \tag{13.25}$$

which is a prediction for connectomic analysis. We note that, by construction, $W^{IE}W^{EI} > 0$. The response time of the system is shortened by a factor of \sqrt{K} , i.e.,

$$\frac{\tau}{\beta} \to \frac{\tau}{\beta\sqrt{K}}O(1).$$
 (13.26)

The change in recovery speed of the network has not been properly measured. But a sudden jump in the excitation of cortical input leads to an observed time-constant of about 10 ms (Figure 6). Unfortunately this is not very different from estimates for isolated neurons and thus the dynamics of the balanced still is a topic under analysis.

Figure 6: Relaxation of the signal in V1 cortical neurons after shut-down of thalamus. From Reinhold, Lien and Scanziani 2015

